



First Test Measurements of a 64k pixel readout chip working in single photon counting mode

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On behalf of the Medipix2 Collaboration*

* See: <http://medipix.web.cern.ch/MEDIPIX/>

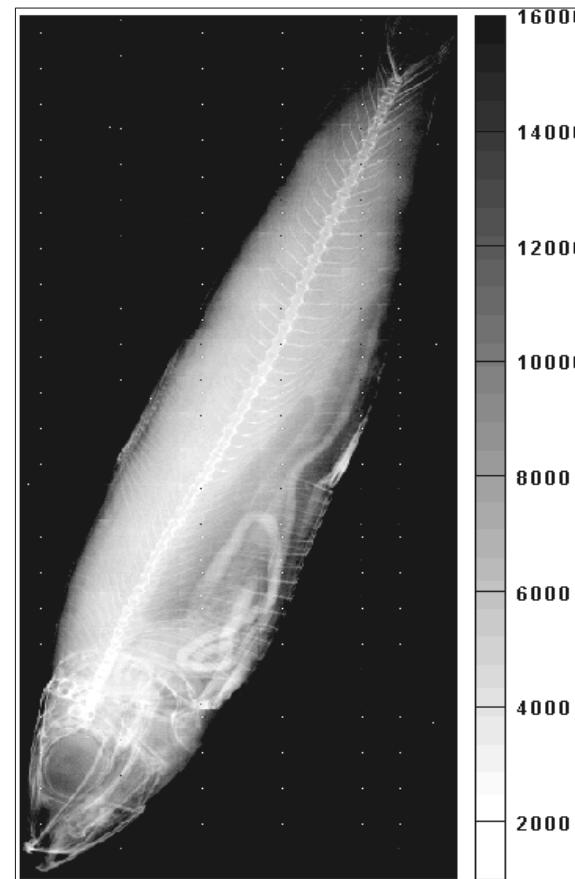


Outline

- ◆ **Introduction**
- ◆ **Motivation for the chip design**
- ◆ **The Medipix2 pixel cell**
- ◆ **The Medipix2 chip architecture**
- ◆ **Electrical measurements**
- ◆ **Conclusions**
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Medipix1 image of a sardine



X-ray tube
Mo target
30 μ m Mo filter
25 kV
5 mAs
50 cm from source
Raw data



Motivations

- ◆ Medipix I proved potential for photon counting pixel detectors.
- ◆ Deep sub-micron CMOS (0.25mm) is available and well characterized.
- ◆ 170 mm to 55 mm pixel side and 64x64 to 256x256 pixels per chip. Pixel dimensions competitive with film-screen systems.
- ◆ More functionality can be added to a smaller pixel.

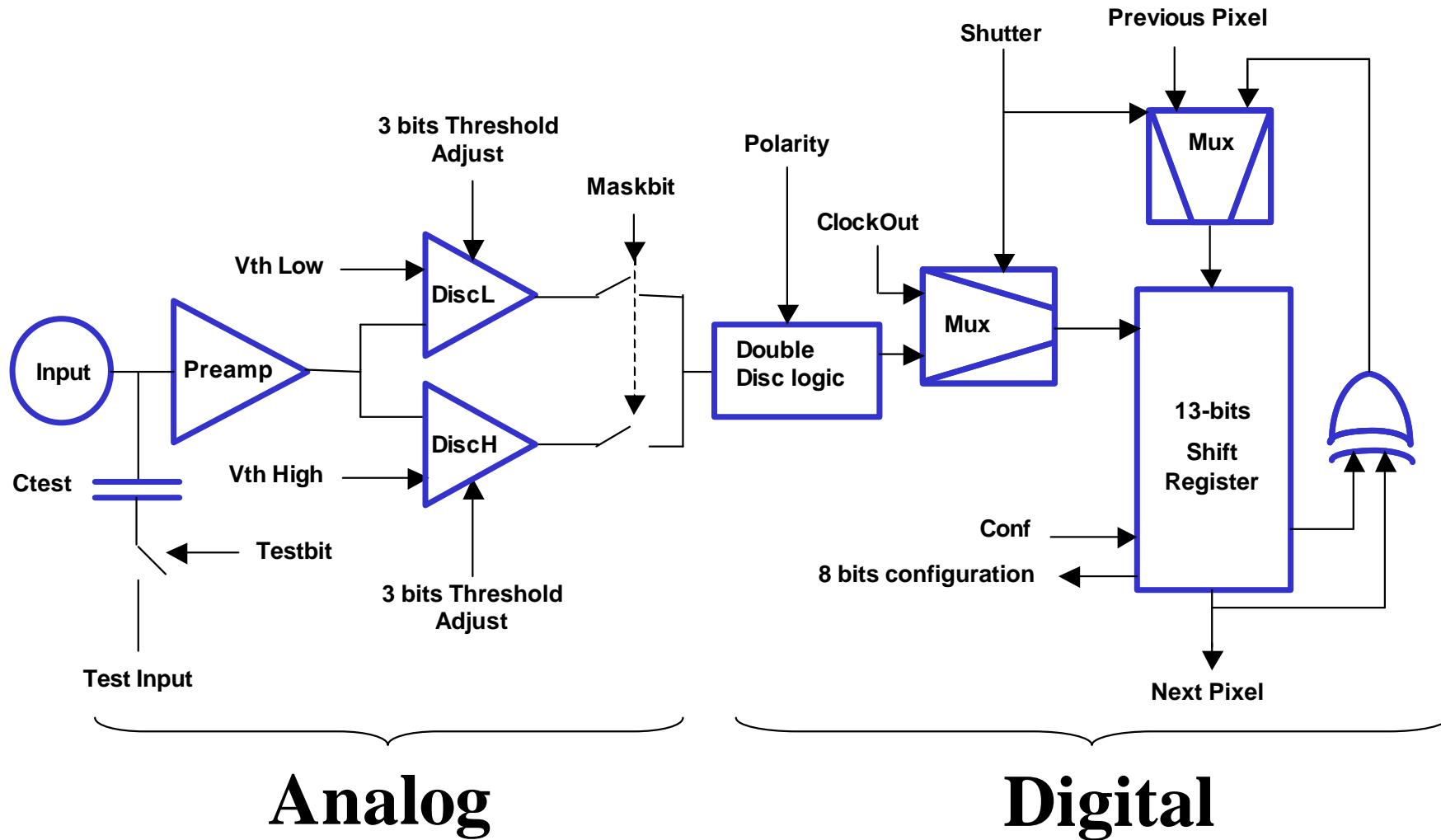


Characteristics of Medipix2 Chip

- ◆ Square pixel size of 55 µm
- ◆ Sensitive to positive or negative input charge (different detector materials can be used)
- ◆ Pixel by pixel detector leakage current compensation
- ◆ Window in energy as precise as possible
- ◆ 13-bit counter per pixel
- ◆ Count rates of 1 MHz/pixel (0.33 GHz/mm²)
- ◆ 256 x 256 pixels
- ◆ 3-side buttable
- ◆ serial or parallel I/O

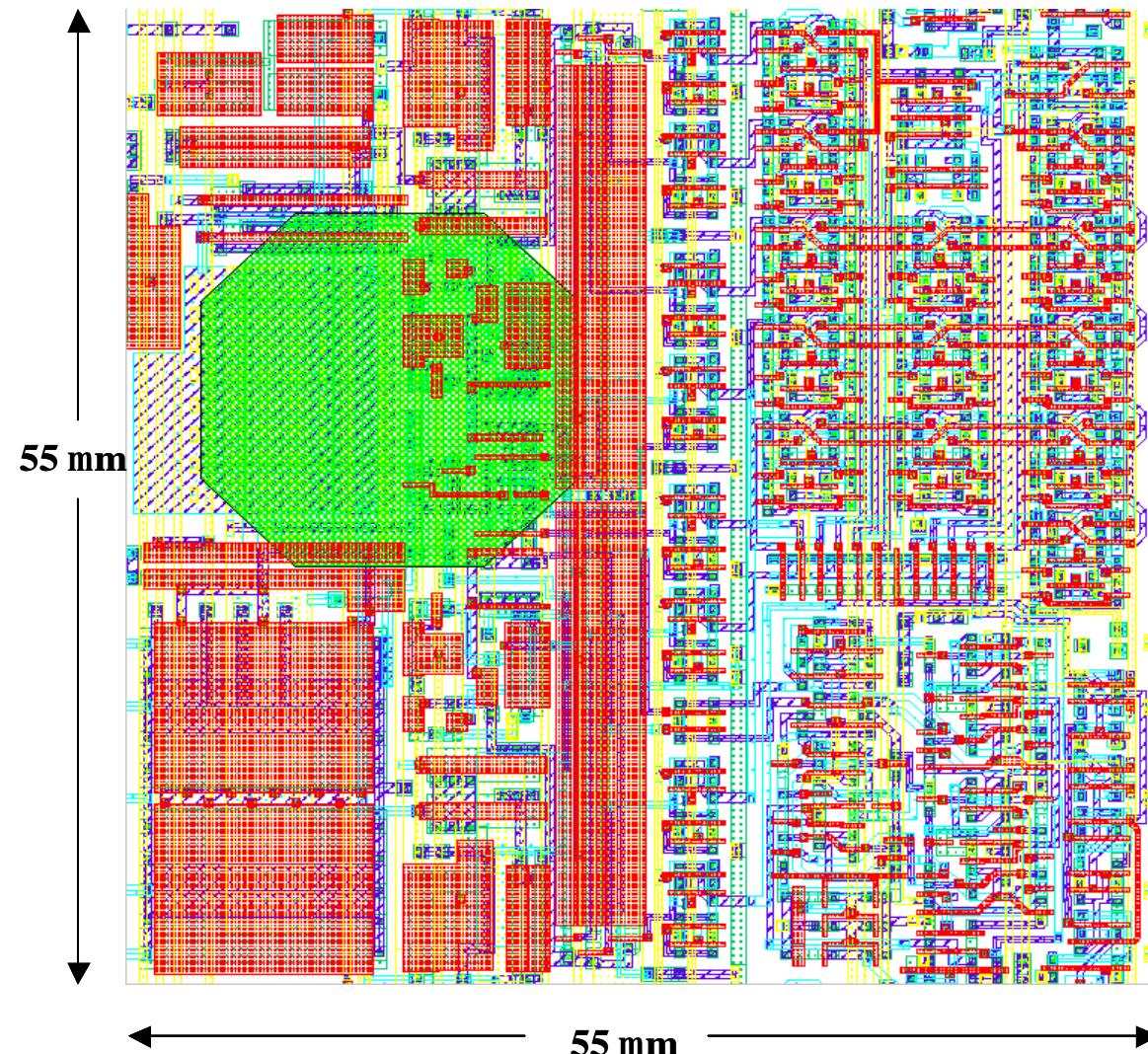


Medipix2 Pixel Cell



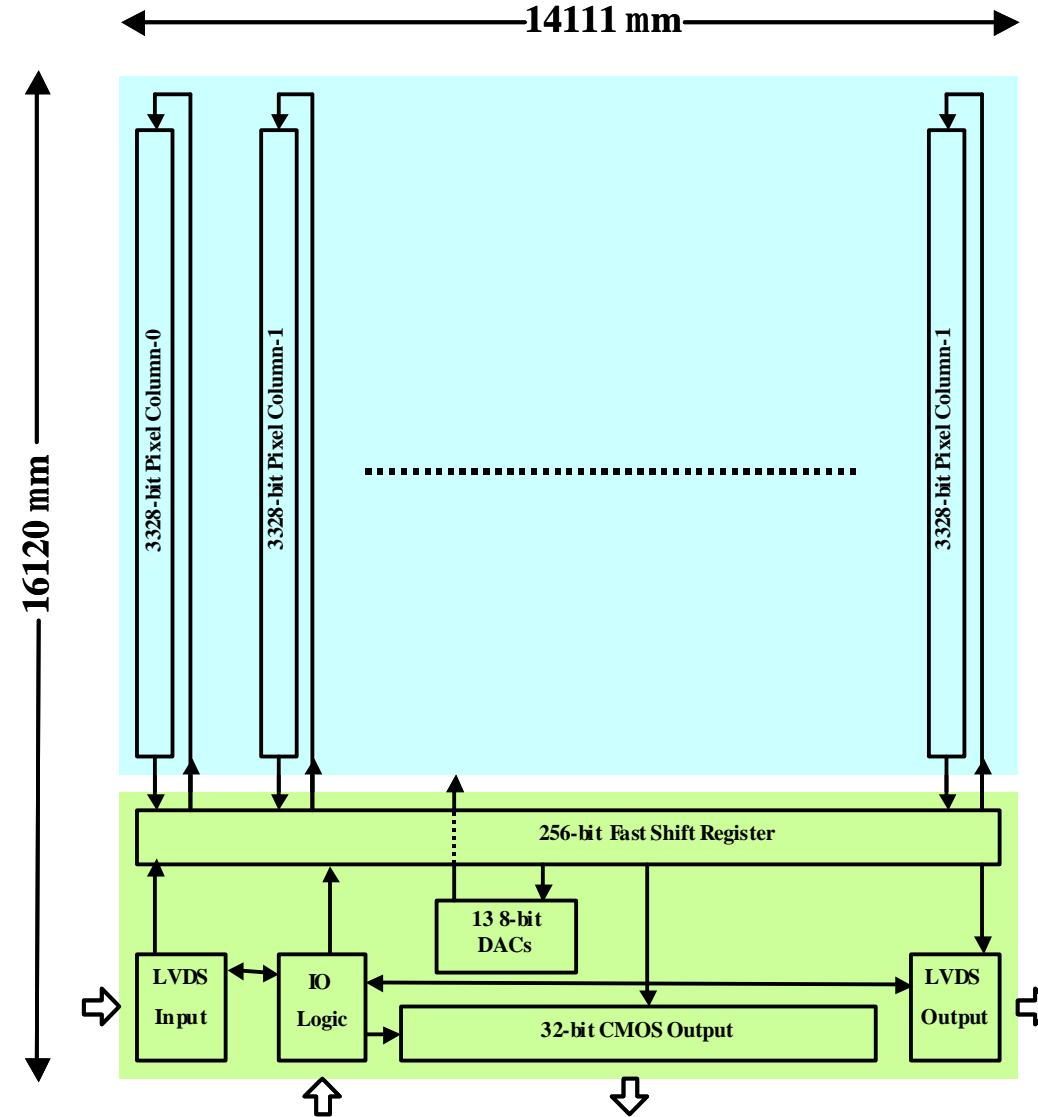


Medipix2 Pixel Cell Layout



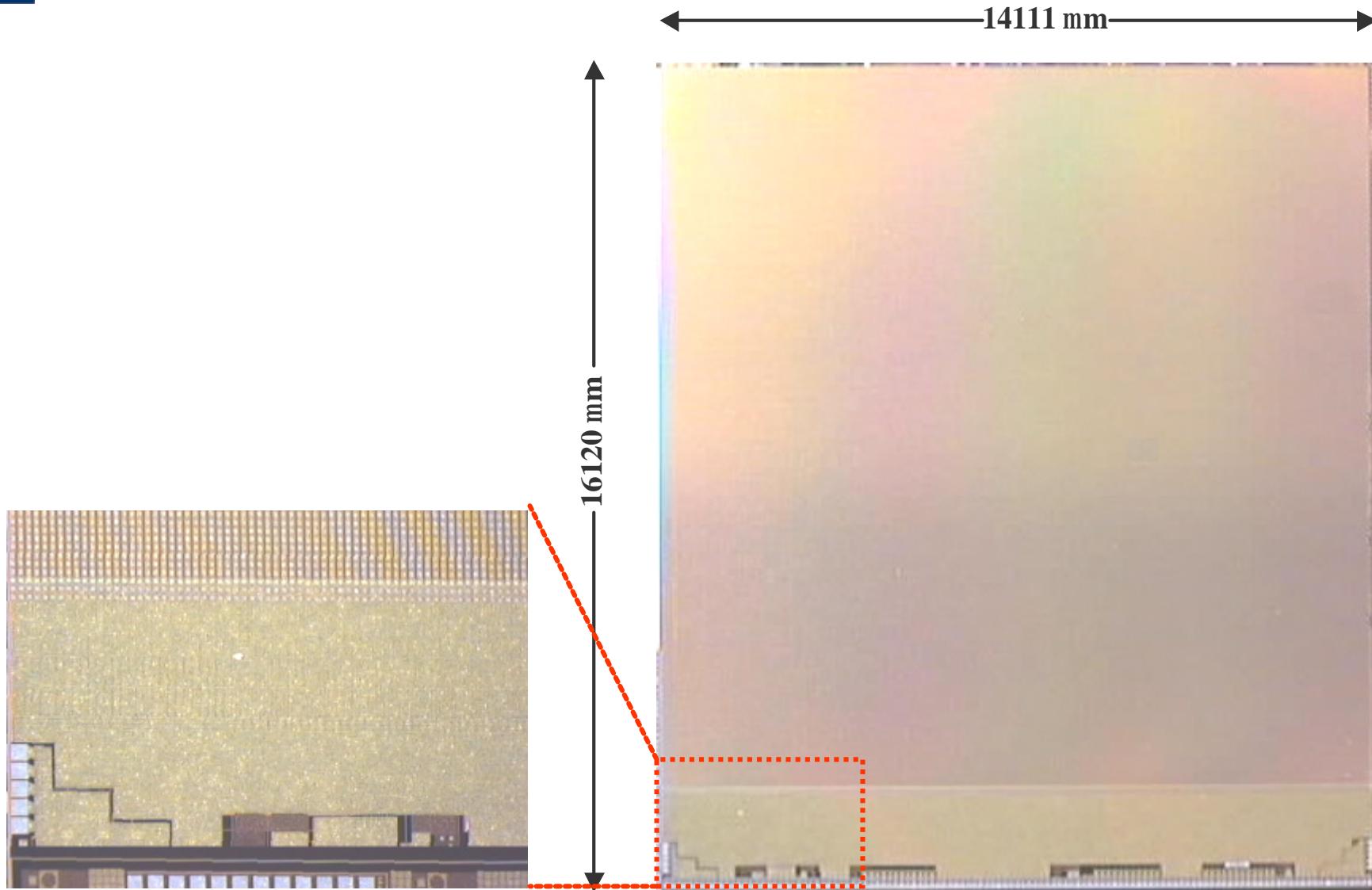


Medipix2 Chip Architecture (I)



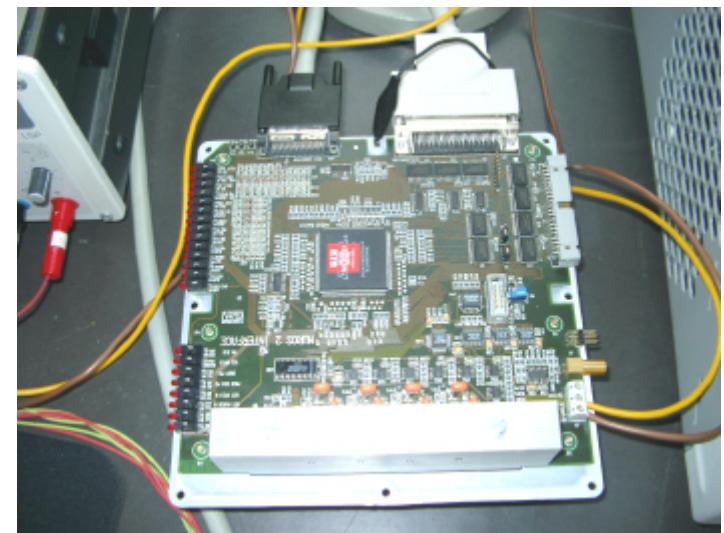
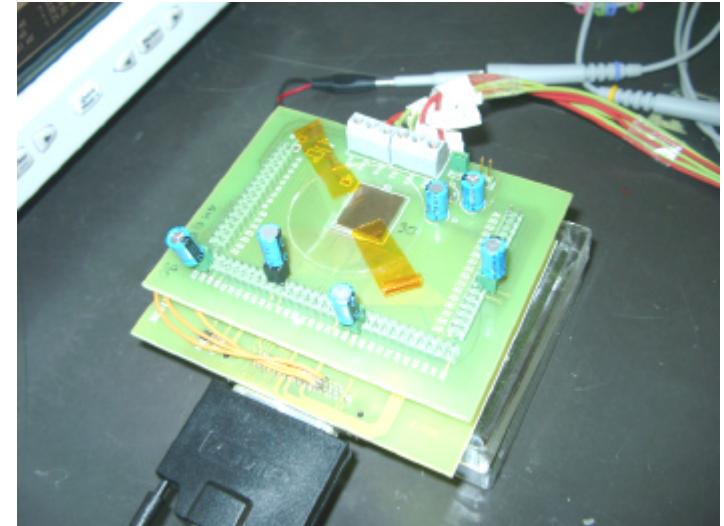


Medipix2 Chip Architecture (II)



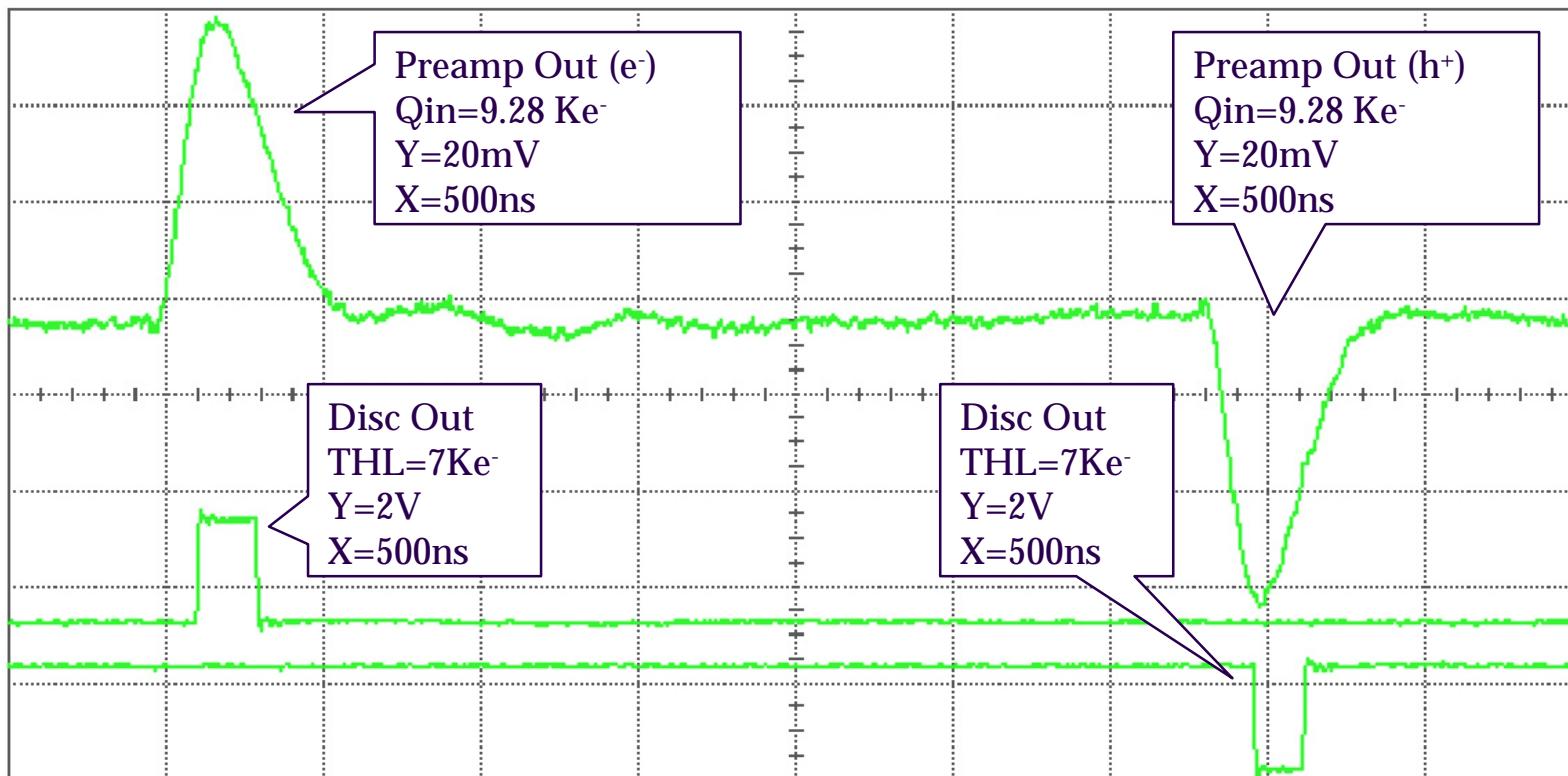


Measurement Setup



Preamplifier and discriminator measurement

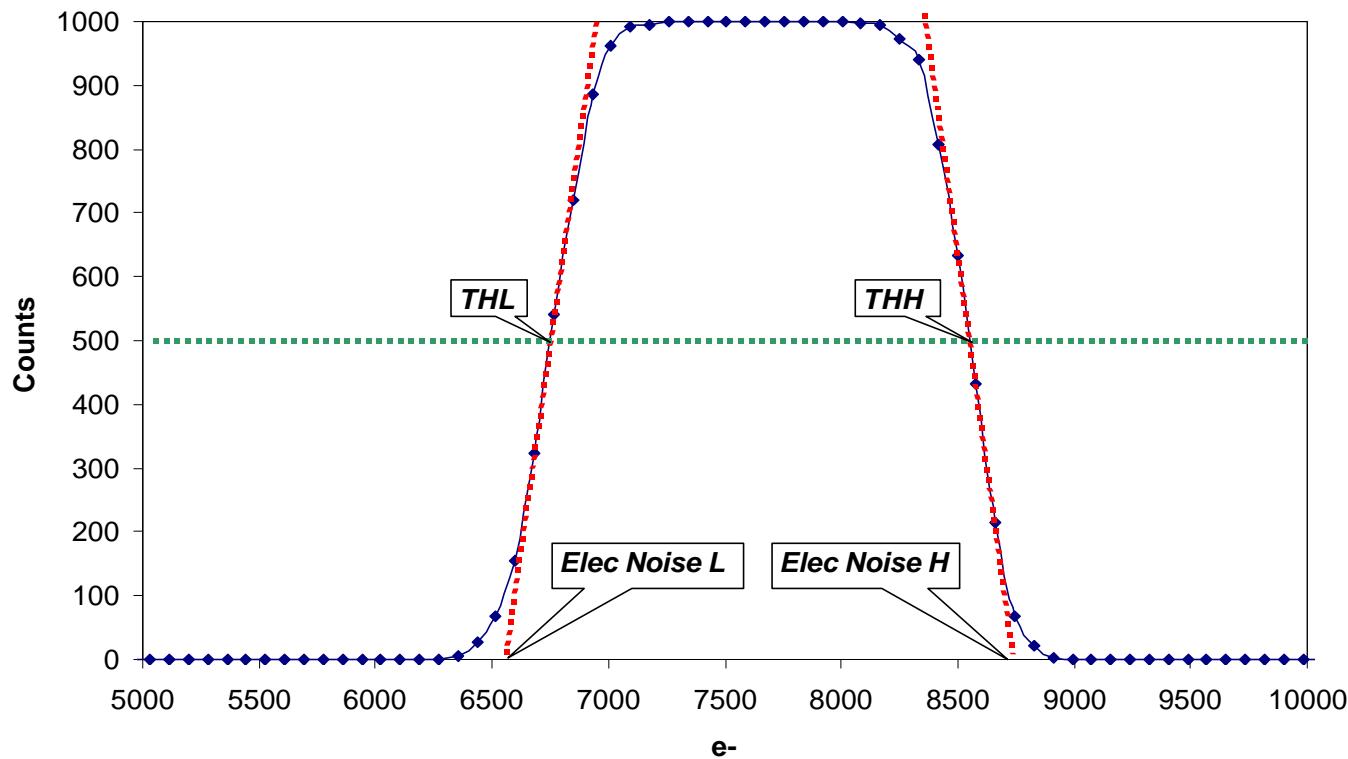
- ◆ Measurements have been done using the Test output Pads and applying a voltage test pulse to the on-pixel injection capacitance.





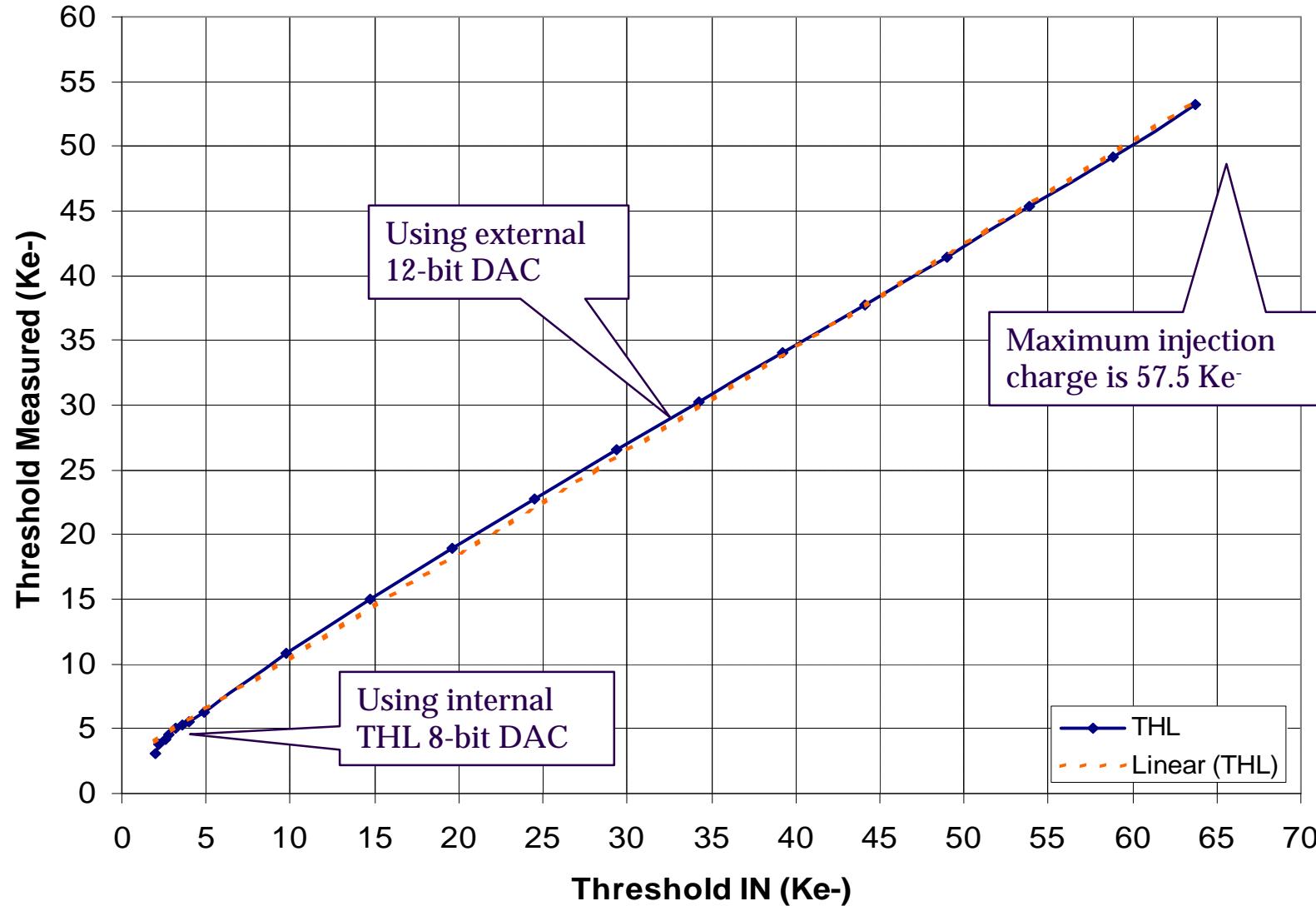
Measurements and Calibration

- ◆ All the reported measurements are done using the electronic calibration (Injection capacitor + external voltage pulse).
- ◆ The 8fF injection capacitor nominal value has a tolerance of 10%.
- ◆ The dedicated Muros2 readout system had been used



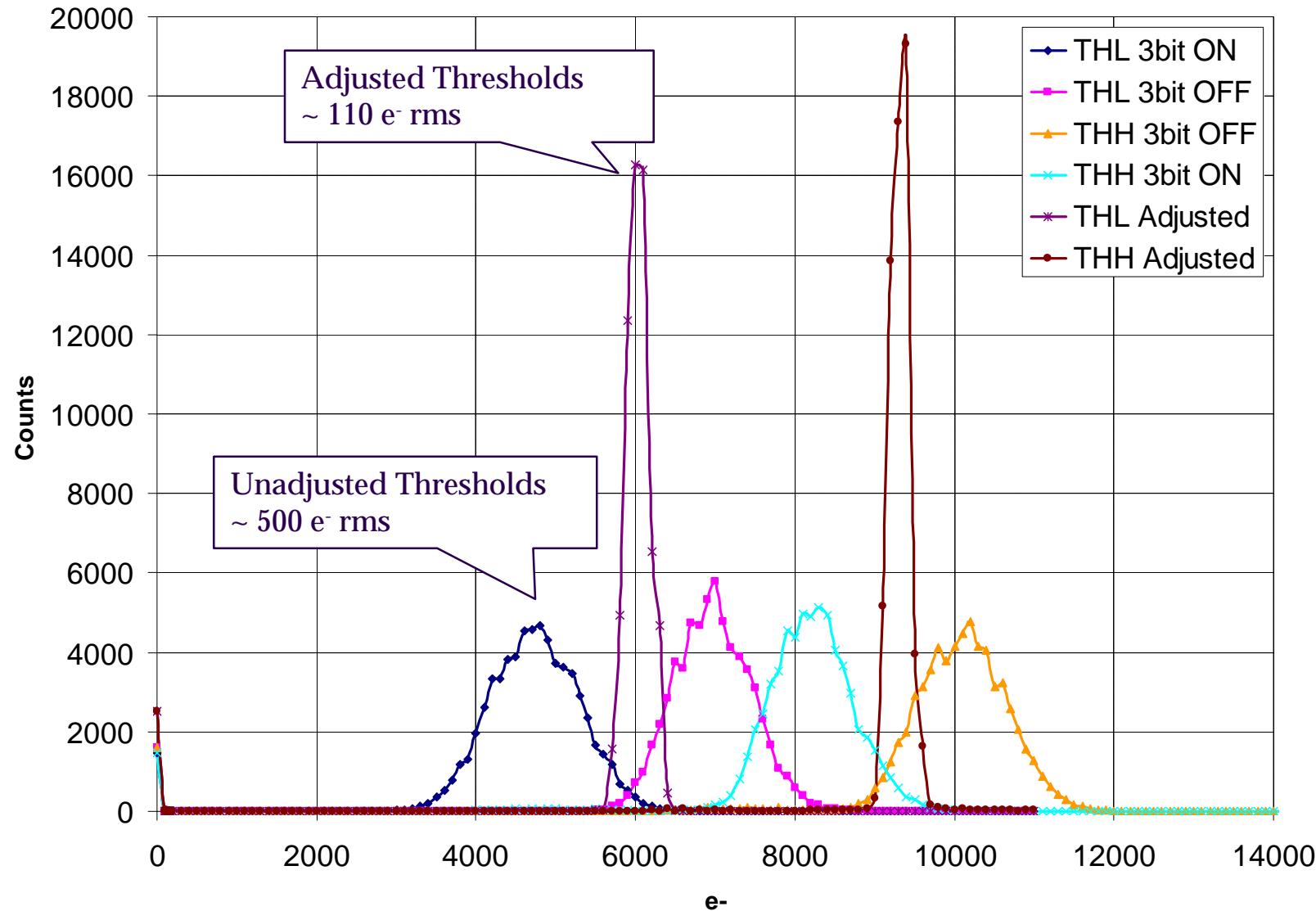


Threshold Linearity



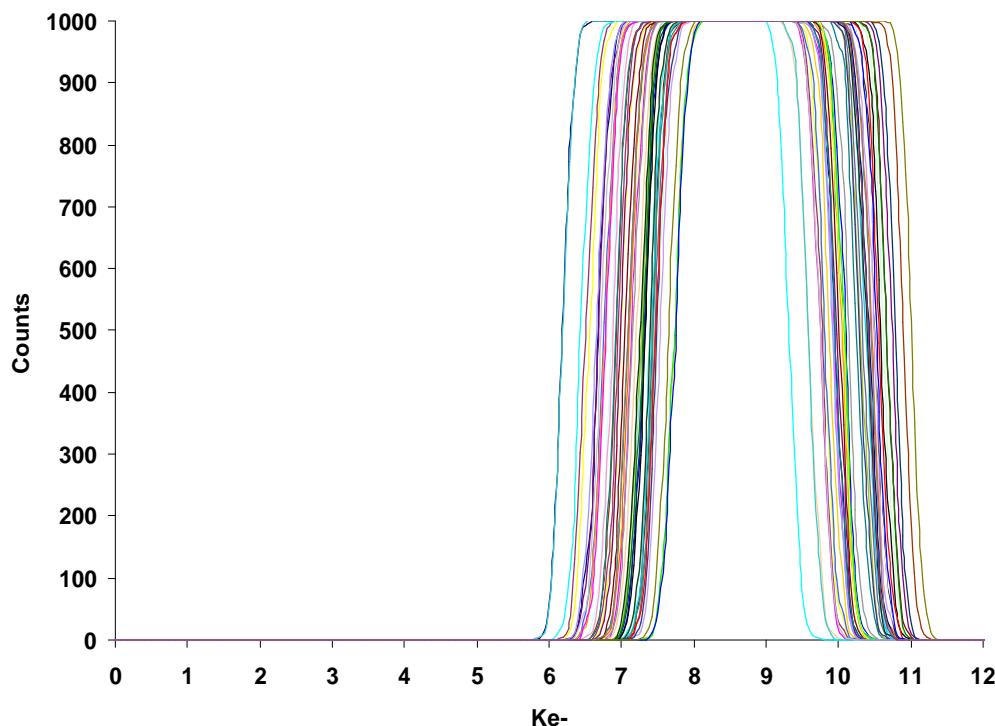


Threshold Equalization (I)

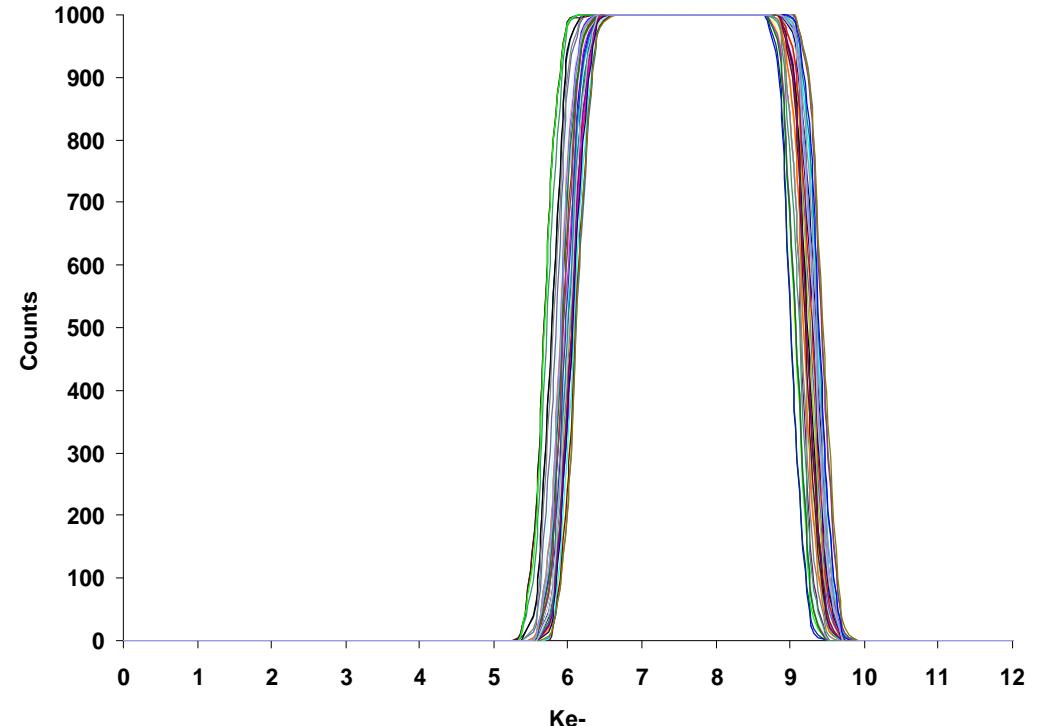




Threshold Equalization (II)



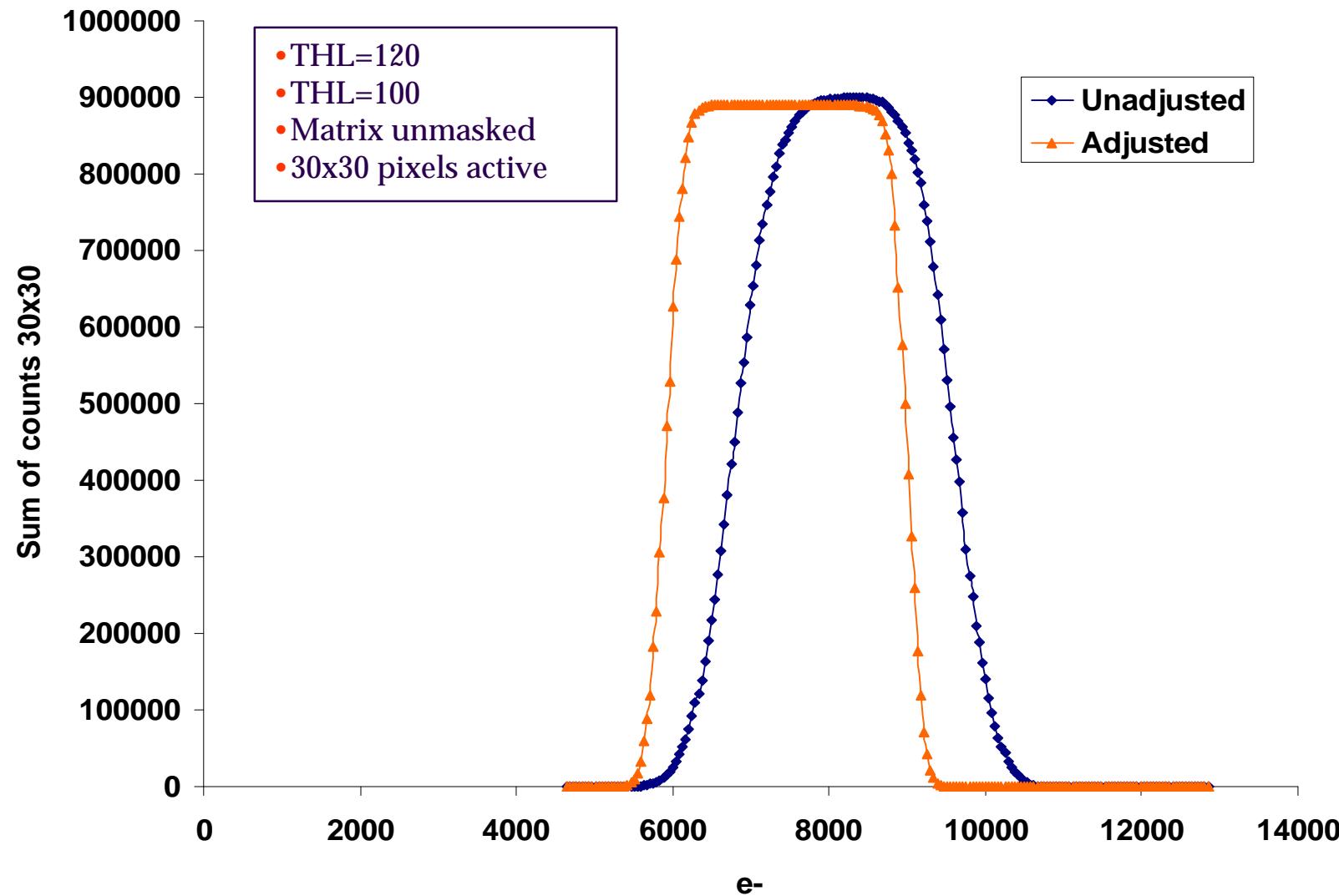
1 row of **Unadjusted** pixels



1 row of **Adjusted** pixels

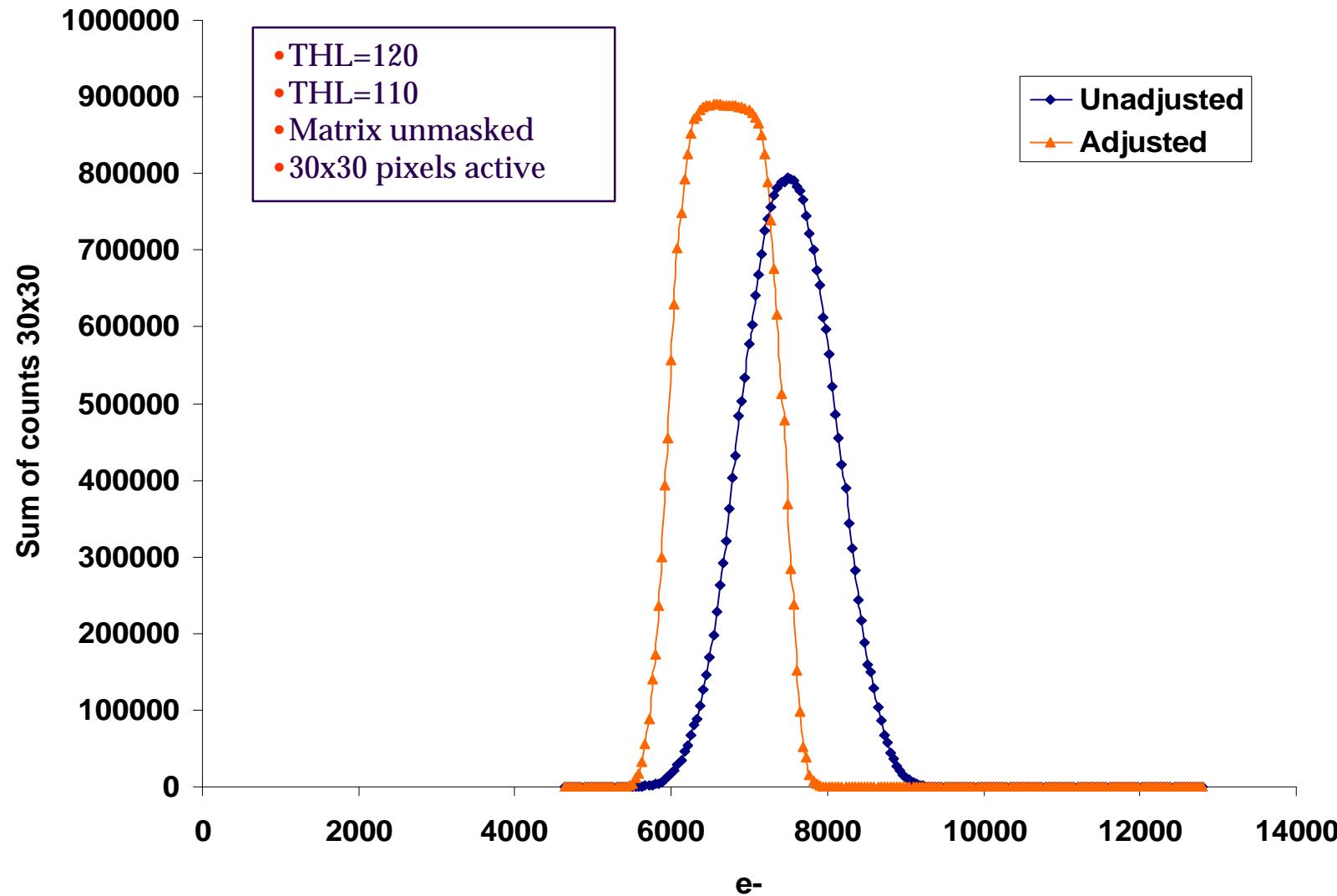


Threshold Equalization (III)





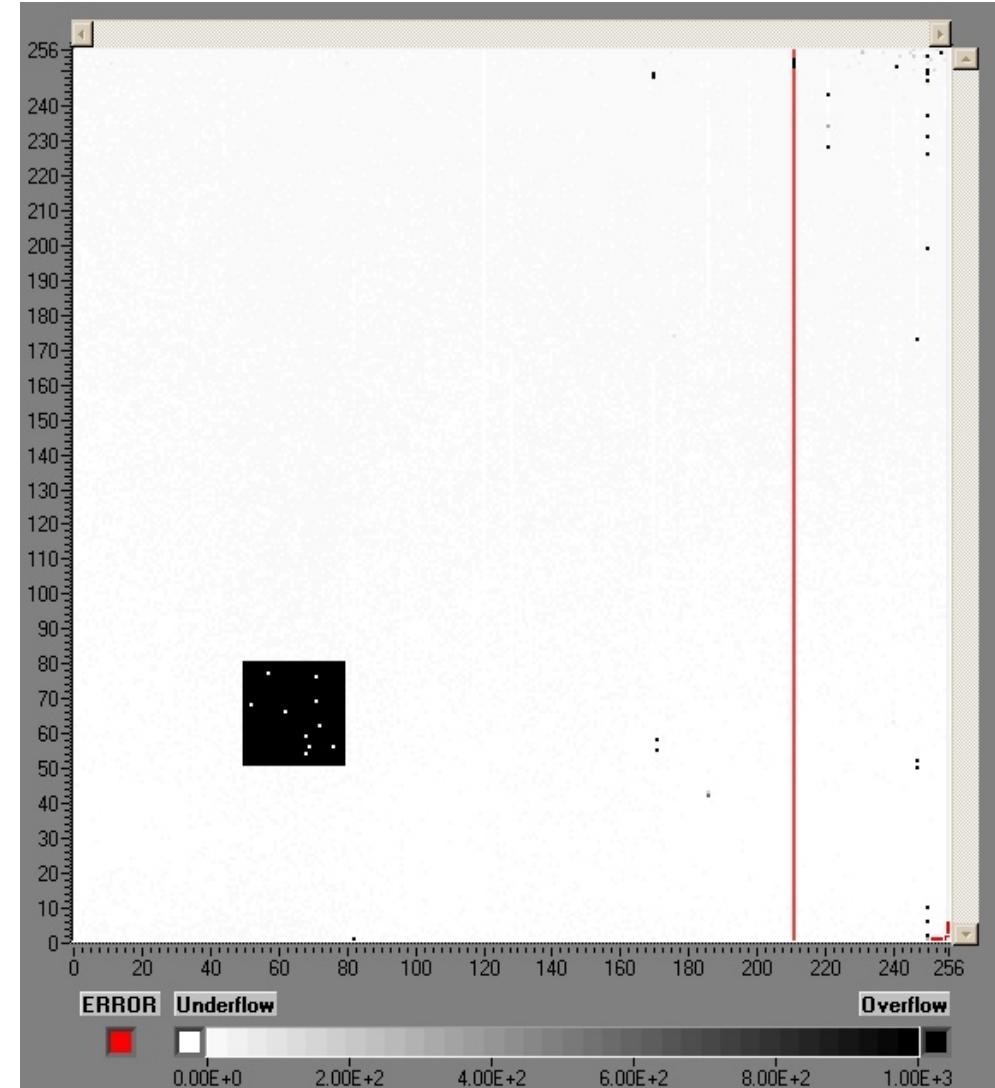
Threshold Equalization (IV)





Threshold Equalization (V)

- THL=140 (2.8 Ke⁻)
- Injection of 1000 pulses of 3.6 Ke⁻
- Matrix unmasked
- 30x30 pixels active





Summary of the Electrical Measurements

	Electron Collection	Holes Collection
Gain	12.5 mV/ke^-	13.25 mV/ke^-
Non linearity	$<3\% \text{ to } 100 \text{ ke}^-$	$<3\% \text{ to } 80 \text{ ke}^-$
Peaking time		$<200 \text{ ns}$
Return to baseline		$<1 \text{ ms for } Q_{in} < 50 \text{ ke}^-$
Electronic Noise		$SnL \sim 105 \text{ e}^- \text{ SnH} \sim 105 \text{ e}^-$
Threshold dispersion		$SnTHL \sim 500 \text{ e}^- \text{ SnTHH} \sim 500 \text{ e}^-$
Adjusted Threshold dispersion		$SnTHL \sim 110 \text{ e}^- \text{ SnTHH} \sim 110 \text{ e}^-$
Analog power dissipation		$\sim 8 \text{ mW/channel for a } 2.2 \text{ V supply}$



Periphery Measurements

- ◆ The 13 DACs perform as simulations
- ◆ Fast shift register works at > 100 Mhz*
- ◆ Peripheral logic works to > 100 Mhz*
- ◆ Serial/parallel I/O work
- ◆ LVDS drivers and receivers work to > 100 MHz*



Radiation Tolerance Measurements

- ◆ 10 keV X-ray source
- ◆ Chip under bias conditions
- ◆ Applied dose rates:
 - ◆ 3.9 krad/min up to 150 krad
 - ◆ 8.04 krad/min from 150 krad to 500 krad
- ◆ Analog power supply current increase from 200mA to 260 mA
- ◆ Digital power supply current increase sharply @ 200 krad reaching 1100 mA @ 500 krad
- ◆ After 1 week of annealing at 100°C the power supplies current recovered to pre-irradiation values
- ◆ Chip showed normal behavior until 200 krad and still functioning after annealing at 500 krad



Conclusions

- ◆ A prototype chip consisting of 256x256 pixels has been produced with a square pixel size of 55 μm . Each pixel has around 500 transistors.
- ◆ Using the dedicated Medipix2 readout system (Muros2 and Medisoft4) complete electronic measurements and threshold calibration have been done.
- ◆ Adjusted threshold variation $\sim 110 \text{ e}^- \text{ rms}$ for both levels of discrimination.
- ◆ Electronic Noise $\sim 105 \text{ e}^- \text{ rms}$.
- ◆ Difficulties to lower the threshold under 2.5 Ke $^-$ with the present setup.
- ◆ The chip is radiation tolerant until at least 200 Krad.



On-going work

- ◆ A new chipboard card is ready to be tested with improved decoupling and power distribution.
- ◆ Probe tested wafers have been sent for bump bonding to silicon detectors.
- ◆ This should allow an absolute calibration with radioactive sources.
- ◆ Other materials will be tried later (CdTe, GaAs, etc...)



Future Prospects

- ◆ With pixel shrinking charge sharing starts to dominate the detector behavior.
- ◆ Hexagonal pixels (on the detector side) become attractive.
- ◆ New front-end electronics architectures are needed.
- ◆ Some ideas are presented in a recently accepted paper for publication in the NSS/MIC IEEE journal.
- ◆ A whole spectrum of new possibilities opens with e.g. time-resolved measurements, very high dynamic range applications, colour X-ray imaging...