



X-ray Scatter-to-Primary Ratio versus Thickness

Two analytic Models Evaluated Against Monte Carlo Calculations

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Outline

- Detectors at GE Research
- Relevance of Scatter/Absorptive Problem To Detectors
- Experimental Data
- Two analytic models
- Comparison to Monte Carlo Calculations
- Conclusions



GE Research

Niskayuna, NY – World Headquarters



Technical Representation

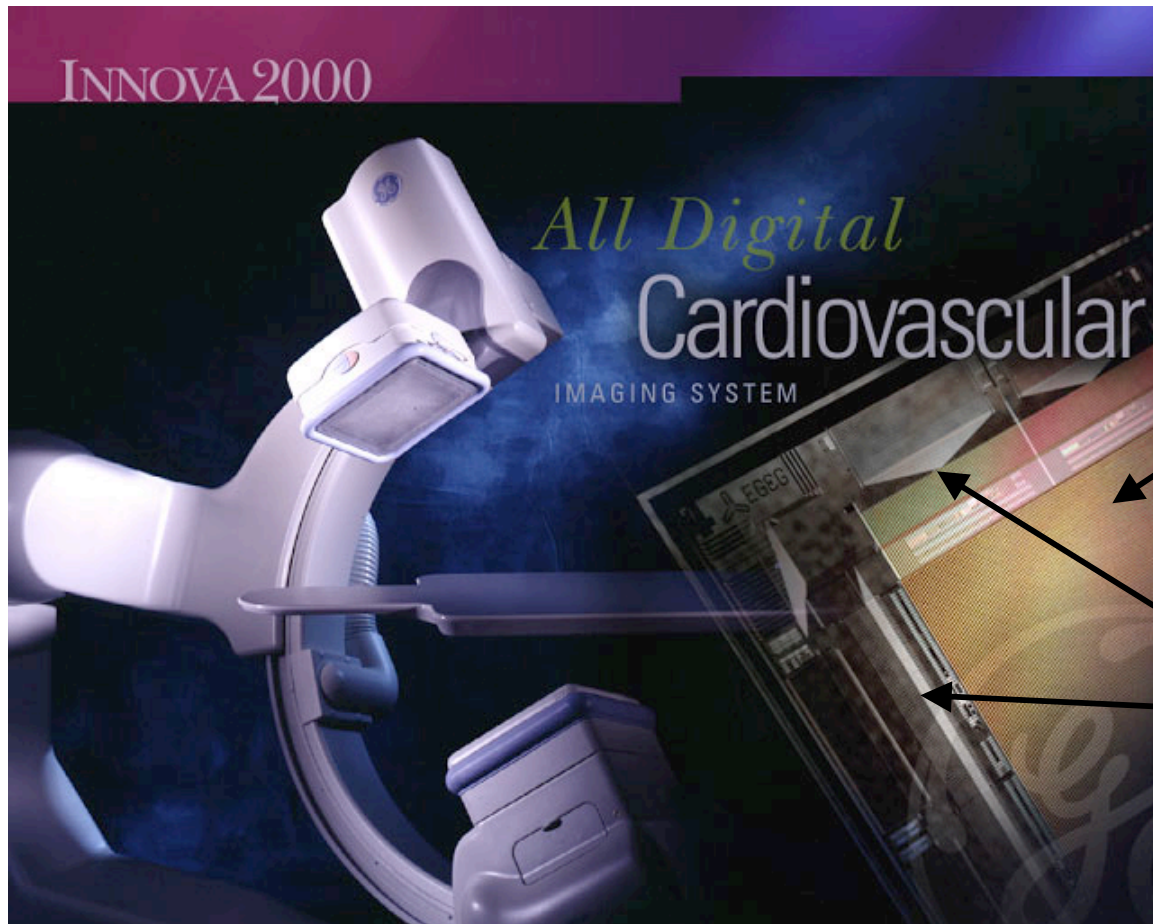
Chemistry	18%
Mechanical	17%
Physics	9%
Electrical	18%
Computer Sci.	17%
All Other	21%



Bangalore, India



Shanghai, China



***CsI Scintillator
on Monolithic Array
of
a-Si Photodiodes
and FET Switches***

***Row & Column
Readout
Electronics***

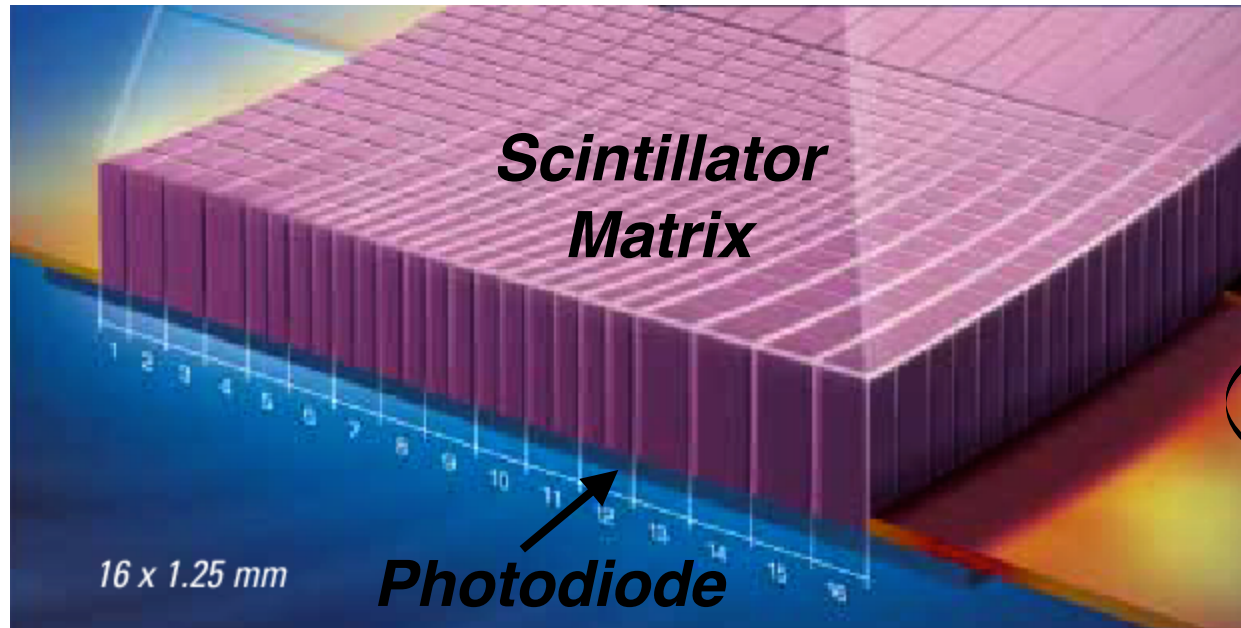
Projected evolution for digital x-ray imaging

- higher resolution pixels***
- greater patient coverage***
- faster scanning***

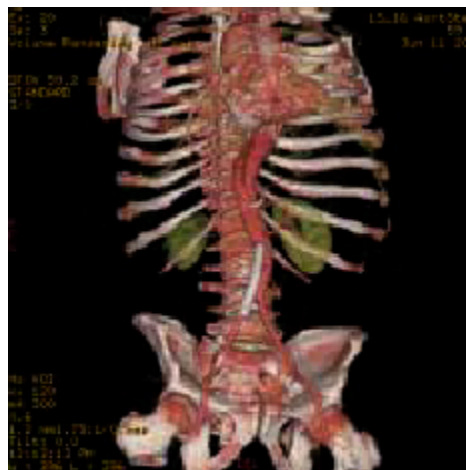
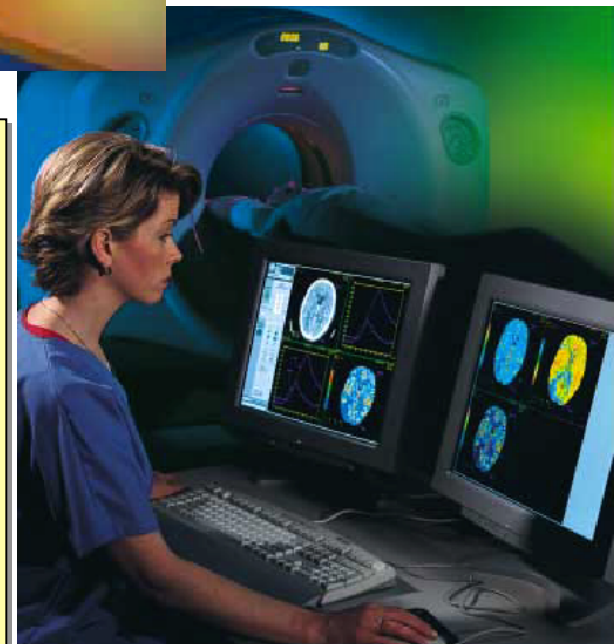


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Multi-slice to Volume CT Detectors



Readout Electronics



Projected evolution is from multi-slice to volume CT

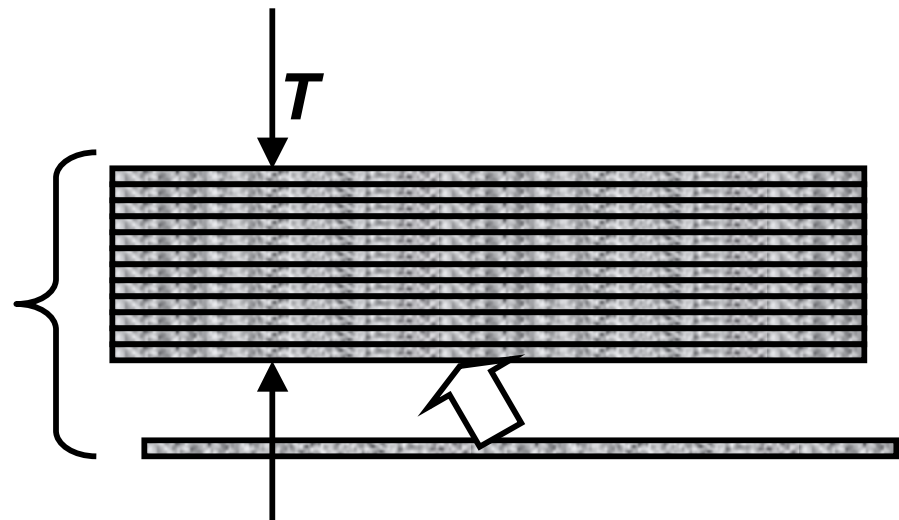
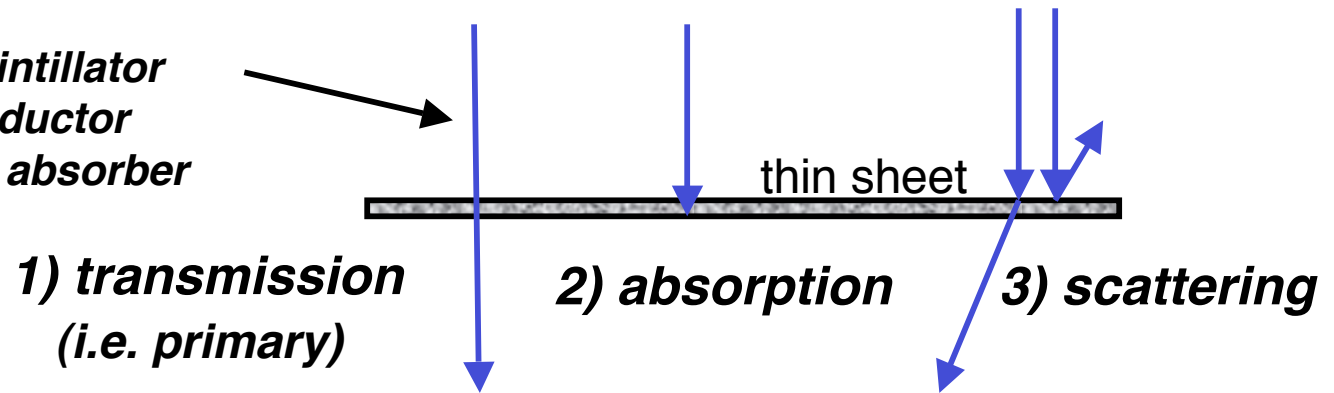
- **higher resolution pixels**
- **much greater patient coverage**
- **faster scanning speed**



Combined Absorption and Scattering Processes

particle of interest could be

- x-ray in patient
- light photon in scintillator
- e/hole in semiconductor
- neutrons through absorber

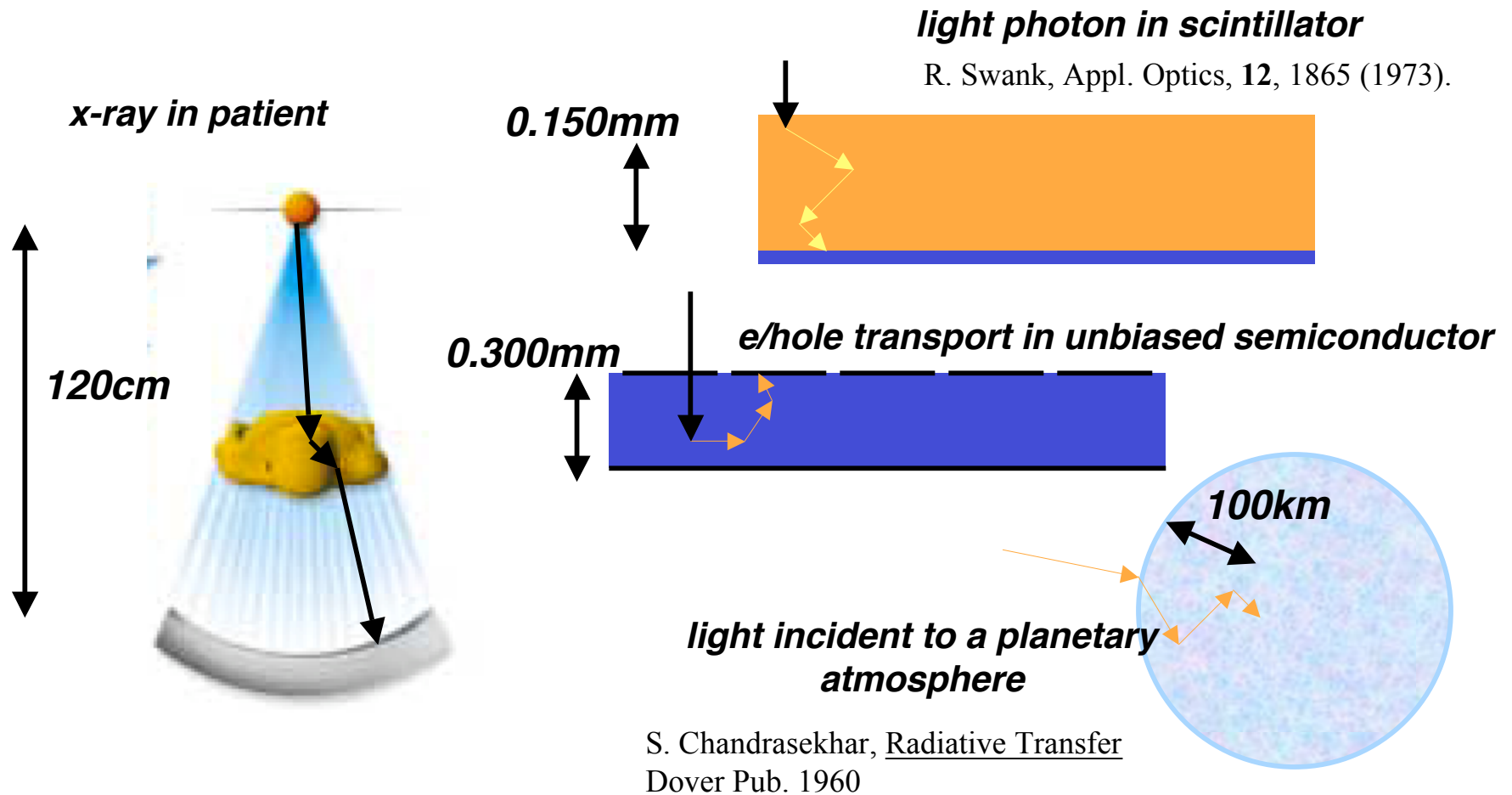


The radiation density profile becomes a remarkably difficult to calculate for non-infinitesimal layers



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Combined Absorption and Scattering Processes



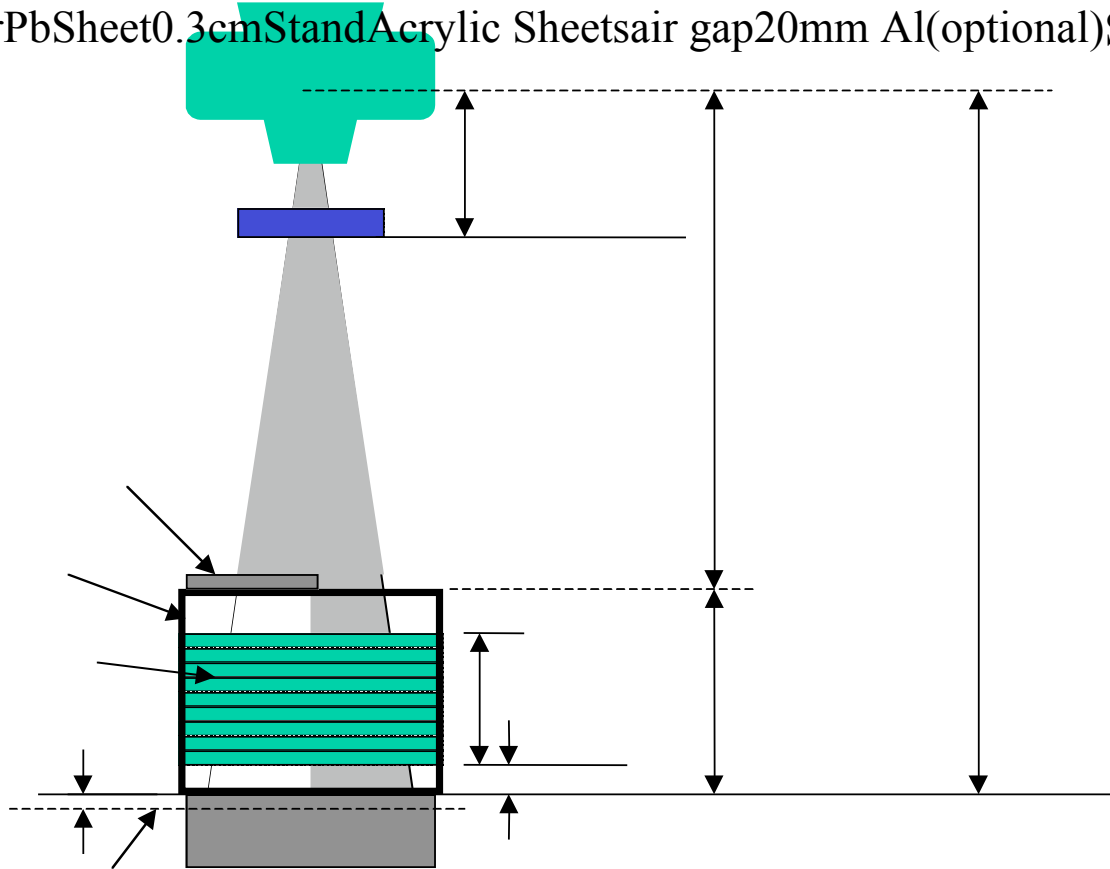
Combined absorption/scatter phenomena is ubiquitous for detectors and imaging.
The albedo = $W = \frac{\sigma_{\text{scatter}}}{\sigma_{\text{total}}}$ is useful to divide the problem space
Detector studies seek to maximize the gain efficiency and minimize crosstalk



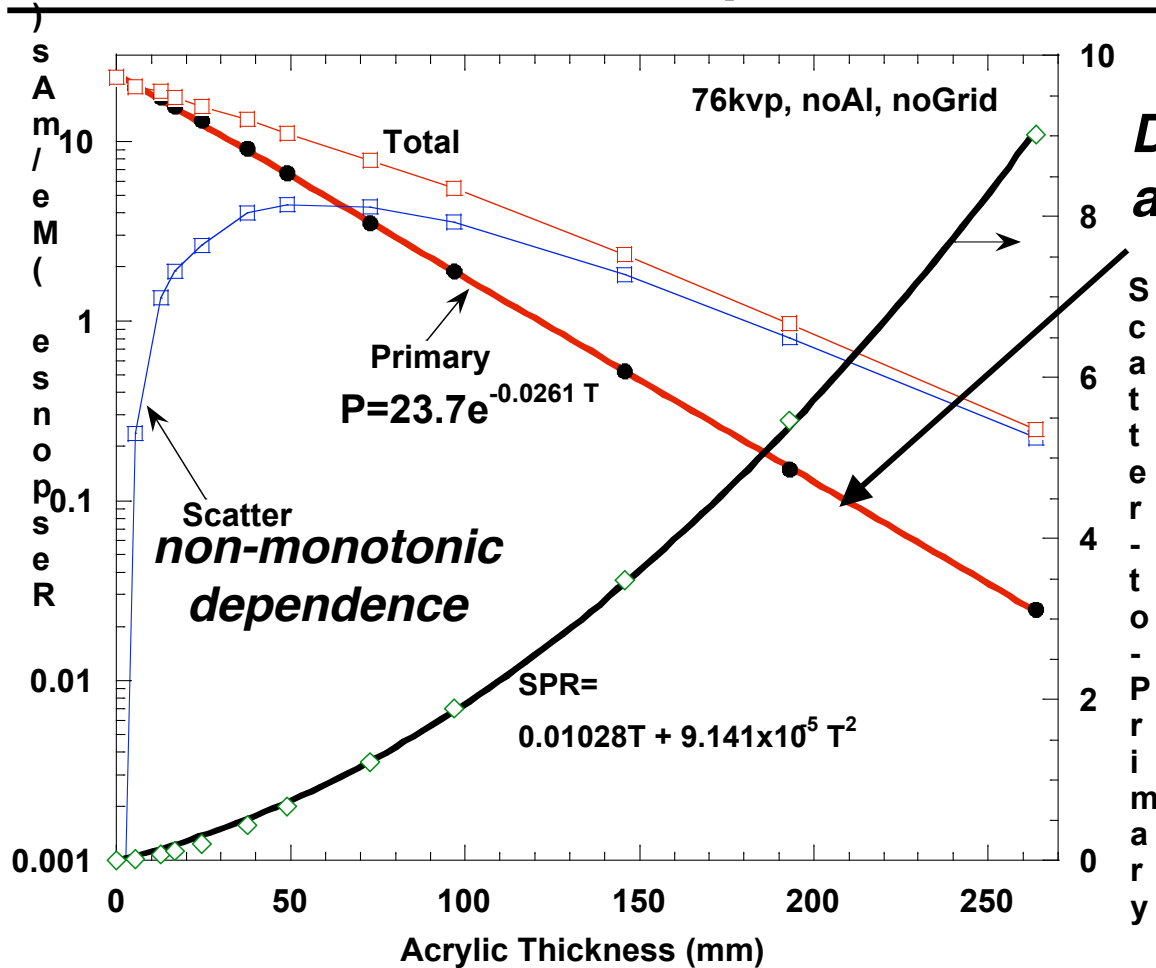
Experimental Study of Scatter



X-Detector Pb Sheet 0.3cm Stand Acrylic Sheets air gap 20mm Al (optional)



- Measurements with and without Pb Sheet Allows Scatter Measurement
- Experimental Results were simulated with MC calculation using GEANT4



Data shows exponential attenuation of the primary

Scatter is non-monotonic ... it is linearly increasing at small thickness and exponentially decreasing at large thickness



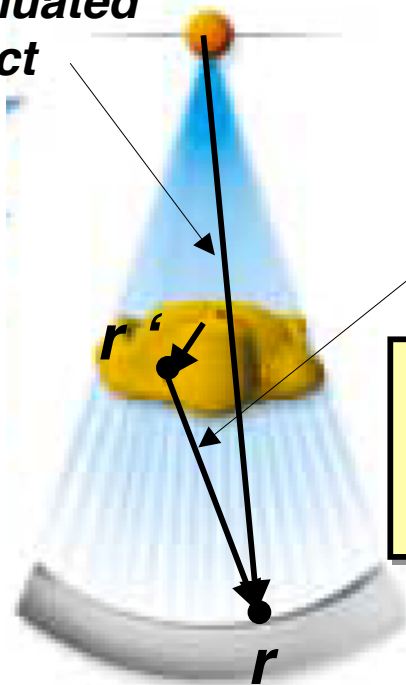
General Formal Solution to the Coupled Scatter/ Absorption Problem is an Integral Equation

S. Chandrasekhar, Radiative Transfer, Dover Pub. 1960

$$I(r, \mu) = \underbrace{I_{source}(0) \frac{e^{-\mu(r,0)}}{r^2}}_{\text{Primary= source attenuated by object}} + \underbrace{\int_V dr' \int_S d\mu' p(\mu_{r'r}, \mu') I(r', \mu') \frac{e^{-\mu(r,r')}}{(r'-r)^2}}_{\text{Scatter from other points in the object}}$$

Primary= source attenuated by object

Scatter from other points in the object



Total Signal is Self-Consistent Sum of Primary from the source and Scatter from all other points



General Solution

$$I(r, \mu) = I_{source}(0) \frac{e^{-\mu r}}{r^2} + \int_V dV' \int_S d\Omega' p(\mu, r, \mu', \Omega') I(r', \mu') \frac{e^{-\mu(r-r')}}{(r-r')^2}$$



conditions of slow variation
(i.e. not valid near surfaces and sources)

A. Ishimaru, Wave Propagation and Scattering in Random Media, Academic Press, Inc. N.Y. 1978.

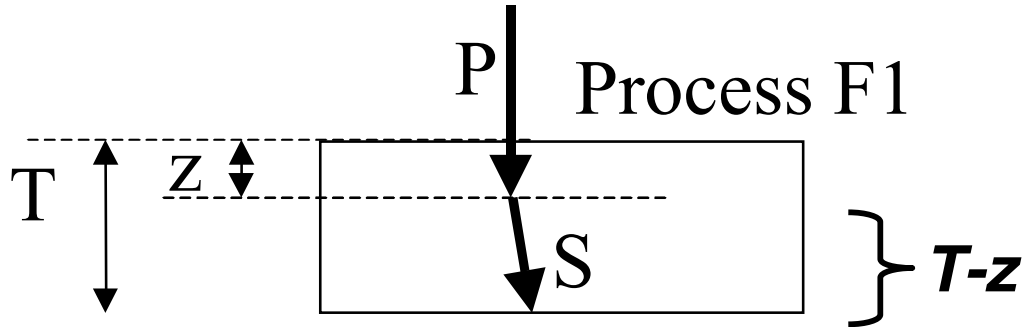
First Order Solution: Diffusion Equation

$$\nabla^2 \phi(r) + \frac{1}{L^2} \phi(r) = S(r)$$

reciprocal diffusion length

source function

Diffusion equation used by Swank to model light propagation in scintillators



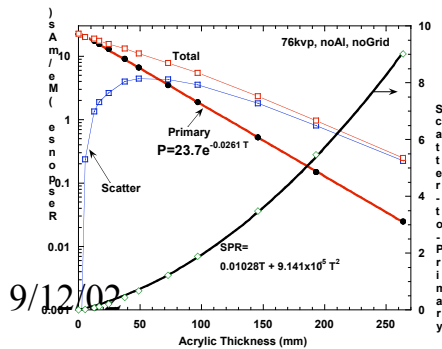
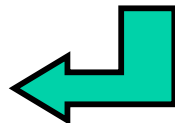
Multiple Scattering is treated by an effective attenuation coefficient for scatter which is less than attenuation coefficient for primary

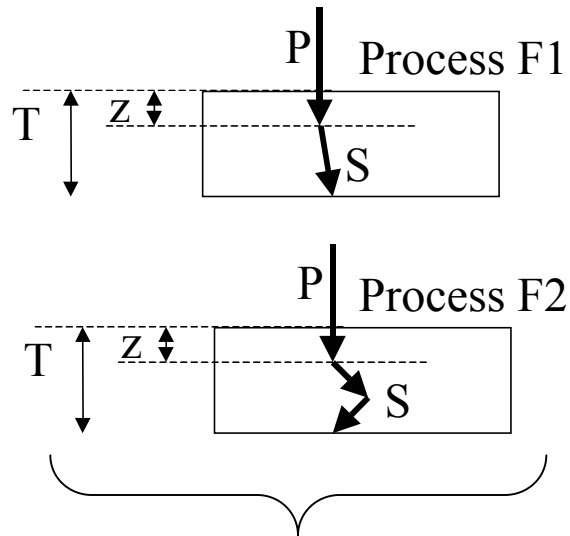
$$\mu_s < \mu_p$$

$$S_F = I_o \int_{z=0}^T dz \frac{\mu_c}{2} e^{-\mu_p z} e^{-\mu_s (T-z)}$$

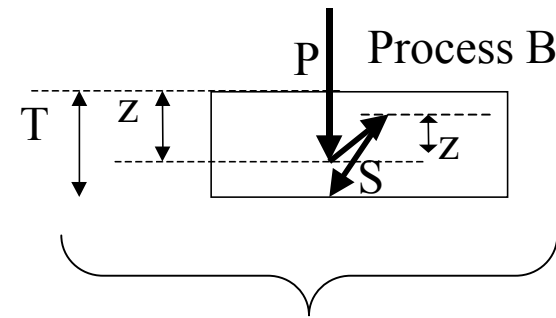
$$= I_o \frac{W}{2(1-\mu_s/\mu_p)} e^{-\mu_p T} \left(1 - e^{-(1-\mu_s/\mu_p)\mu_p T} \right)$$

describes the observed non-monotonic dependence





“1st Forward Scatter”
included by Smith & Kruger



“1st Back-Scatter”
added for more complete treatment

[1] S.W. Smith and R.A. Kruger, “A signal processing model of diagnostic x-ray scatter,” Med. Phys. 13, 831 (1986).

Augment the Method of Smith and Kruger
by including Back-Scattered Processes



Smith and Kruger model extended to include backscatter

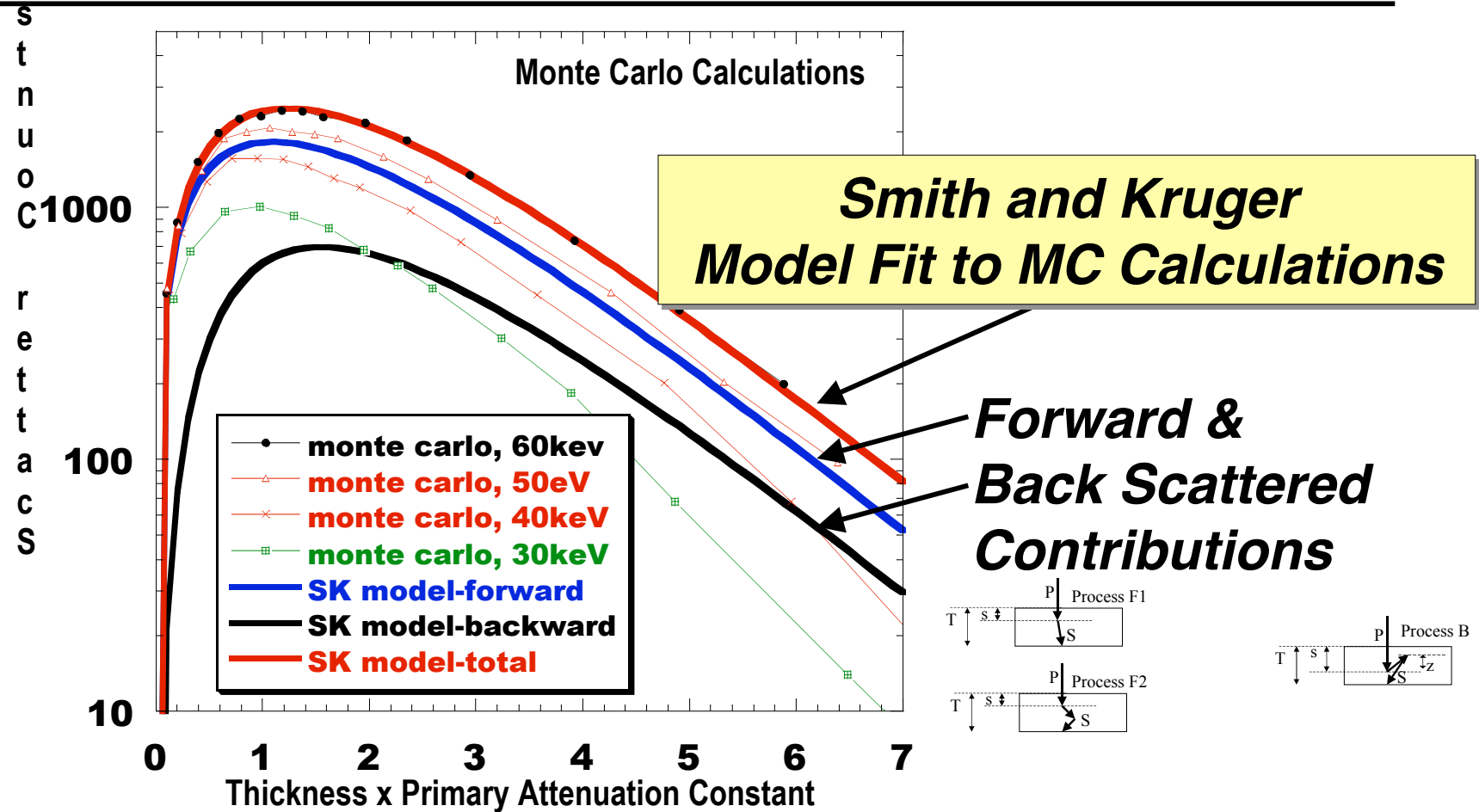
$$S_T = I_o \frac{W}{(1+\mu)} e^{-\mu W} p^T \frac{1 + (1+c)\mu}{1+\mu} + \frac{(1+c/2)(1+\mu)}{1+(1+c)\mu} e^{-\mu(1+\mu)W} p^T + \frac{c}{2} \frac{1+\mu}{1+\mu} \frac{1+\mu}{1+(1+c)\mu} e^{-\mu(1+\mu)W} p^T$$

Diffusion equation for slab geometry with perpendicular incidence.

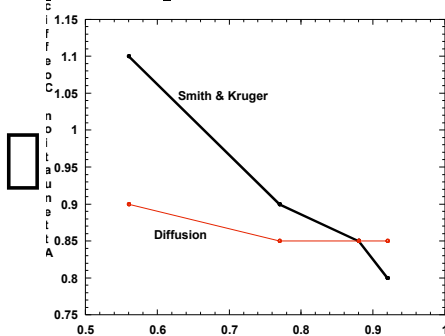
$$S_T = I_o \frac{W/2}{(1+\mu)} e^{-\mu W} p^T \frac{4\mu(1+\mu)}{(1+\mu)^2(1+\mu)} + \frac{(1+\mu)(1+\mu)}{2(1+\mu)} e^{-\mu(1+\mu)W} p^T + \frac{1}{2} \frac{1+\mu}{1+\mu} (1+\mu) e^{-\mu(1+\mu)W} p^T$$

R.K. Swank, "Calculation of Modulation Transfer Function of X-ray Fluorescent Screens,"
 (equation 23 was used), Appl. Optics, 12, 1865 (1973)

What is striking about this comparison is the similar exponential dependences obtained from such different approaches
 The parameter μ appears in both expressions and represents the relative attenuation of scatter compared to primary



key	Monte Carlo Params				1D model Fits		Diffusion Model Fits			
	photo	electron	total	albedo	?	c	?	?	expected	expectec
30	0.1410	0.183	0.324	0.56	1.1	0	0.9	0.2	1.14	0.847222
40	0.0543	0.184	0.238	0.77	0.9	0.0	0.85	0.4	0.83	1.157773
50	0.0265	0.187	0.213	0.88	0.85	0.5	0.85	1.0	0.61	1.31338
60	0.0151	0.181	0.196	0.92	0.8	1.0	0.85	3.0	0.48	1.384439



Albedo

Final fit parameters

Conclusion

- Fits to the analytic model to the MC calculation relates parameters in the analytic model to cross-section for scatter and absorption**
- Models can be used in studies of scintillator and photodiode performance**